Inferior vena cava filters: A contemporary review

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Thromboembolic disease constitutes a wide range of diseases, including deep vein thrombosis (DVT) and pulmonary embolus (PE), and is a common cause of death in hospitalized patients in the United States. According to a study in 2006, the incidence of DVT in the United States ranges from 250,000 to 20 million cases per year, most of which require treatment or hospitalization for lower extremity DVT. PE is the third leading cause of death in the United States and the annual incidence of acute pulmonary embolic events is 600,000 cases.1

Deep venous thrombosis generally develops within the deep veins of the lower extremities, but it can arise from pelvic or even upper extremity veins. In the mid-19th century, Virchow explained the etiology of DVT to include the triad of venous stasis, intimal injury, and hypercoagulability. Thus, risk factors for DVT include, but are not limited to, prolonged immobilization, such as with prolonged travel and after surgery, hypercoagulable states, neoplasm, pregnancy, and estrogen therapy. Genetic predisposition and advanced age (>50) are also associated risk factors. Once a thrombus is formed in the deep veins of the body, it is susceptible to embolizing into the pulmonary arteries.

Systemic anticoagulation is the therapy of choice for all forms of DVT, and initiation of therapy can reduce the mortality rate from 30% to 8%,2 making PE one of the most preventable causes of in-hospital mortality. Common pharmacological agents utilized include heparin and warfarin. However, anticoagulation may be contraindicated in a subgroup of patients due to several reasons, including bleeding diathesis, active bleeding, recent major surgery, intracranial neoplasm, hemorrhagic stroke, and pregnancy. In these patients, placement of an inferior vena cava (IVC) filter is considered as an alternative in the prevention of PE. Additionally, IVC filters are indicated for patients who develop recurrent DVTs and/or PEs while on anticoagulants. Prophylactic use of IVC filters has also been advocated for patients at high risk for thromboembolic events, such as patients with chronic pulmonary hypertension.

After proper clinical evaluation of the patient, additional laboratory and imaging studies are often required for complete evaluation prior to IVC filter placement. The presence of lower extremity DVTs can be assessed with ultrasound and peripheral venography. Pulmonary embolus is diagnosed with either a computed tomography (CT)
scan or a ventilation-perfusion (VQ) scan. When available, CT or magnetic resonance imaging (MRI) is used for anatomic evaluation of the IVC to determine size, configuration, and anatomic variations. However, inferior venocavography, performed in an interventional imaging suite, is almost always utilized prior to filter placement. Laboratory tests, including prothrombin time, activated partial thromboplastin time, INR, and serum BUN/creatinine levels are also routinely obtained as part of initial evaluation.

After introduction of the first IVC filter in 1973, several types of permanent and temporary filters have been developed. Historically, subsequent filter designs were made to improve upon their predecessors. Structurally, the filter should be durable, made of a biocompatible material that is non-corrosive and nonthrombogenic. Also, it should be easily deployable, but it should not easily migrate and not perforate the IVC or adjacent tissues.

When deciding which IVC filter to use, several important qualities of the filter must be evaluated. These include its inherent physical properties, clot-trapping effectiveness, ease of placement, and ability to preserve blood flow in the IVC. Ideally, a filter should trap most, if not all, thrombi to prevent PE. Even with incomplete deployment of the filter, reasonable clot trapping ability is desired.

IVC filters are generally effective when indicated. A comprehensive review of permanent IVC filters reported an incidence of recurrent PE ranging from 2.6% to 3.8% with fatal PE being less than 2%. However, complications have been widely reported and must be routinely considered. Available data on efficacy and complications rates of retrievable filters are relatively sparse when compared to permanent filters, and no single head-to-head comparison of both classes of filters has been made to date. This review summarizes the general description, characteristics, efficacy, and complication rates of both permanent and temporary (retrievable/optional) inferior vena cava filters reported in the medical literature to date.

**Permanent IVC filters**

Seven types of permanent IVC filters are described—all developed to replace surgical ligation clips and IVC clips in the prevention of PE. All are approved by the FDA. With few exceptions, most are generally introduced via the right internal jugular (IJ) or femoral vein. Most share similar complication rates (some more or less than others), including: damage to IVC and adjacent tissues, IVC thrombosis, insertion site thrombosis, filter migration, and filter limb fracture (Figures 1-8).

**Stainless steel Greenfield filter**

The Greenfield filter is the most extensively reviewed and evaluated permanent filter. Introduced in 1973, this filter is made of stainless steel. It is conically shaped with the apical hub pointing cranially, and 6 stainless steel legs radiating caudally (Figure 9A). Although the initial filter was introduced via a 24F catheter, a smaller 12F delivery system was later developed and approved by the FDA in 1995. The efficacy of this filter has been reported by multiple authors. Greenfield, et al., reported only a 4% recurrence rate of PE out of 642 filters placed over a 20-year period. However, complications have been widely reported and must be routinely considered. Available data on efficacy and complications rates of retrievable filters are relatively sparse when compared to permanent filters, and no single head-to-head comparison of both classes of filters has been made to date.

**Titanium Greenfield filter**

Introduced in 1989 as a lighter, nonferromagnetic, nonthrombogenic version of the Greenfield, this filter is made of titanium alloy and is also conically shaped with 6 radiating limbs (Figure 9B). The use of titanium permits resistance to flexion and corrosion. Efficacy rates similar to its stainless steel counterpart have been reported. Greenfield and Proctor demonstrated a 2.9% recurrence rate of PE in 373 patients observed over 13 years. However, higher filter tilt, migration, penetration, and crossing of filter struts have been reported with the Titanium Greenfield filter (Figure 1).

**Vena Tech-LGM filter**

Originally designed in France, this filter was approved by the FDA in 1989. It is composed of a nonferromagnetic (MRI compatible) metallic alloy called Phynox. This filter is also shaped like a cone with 6 limbs that radiate from the apex. Additionally, however, obliquely angled side rails are attached to each limb, which provides stability to the filter once it is deployed in the cava (Figure 9E). It is delivered via a 12F sheath. A key problem with this filter is occasional incomplete opening following deployment, especially when placed via the jugular approach. This results in decreased clot trapping and higher rates of filter thrombosis, decreased IVC patency, and recurrent PEs.
Vena Tech-LP filter

The Vena Tech-LP was a new design approved by the FDA in 2001. It is also made from the nonferromagnetic metallic alloy, Phynox. However, unlike the LGM design, it is made of 8 wires attached to 4 sets of inverted V-shaped adhering limbs (Figure 9C). It is introduced with a 9F sheath; thus, it is small enough to be placed via the antecubital approach in addition to IJ and femoral venous approaches. Reports of efficacy and complication rates are still pending for this relatively new filter design.

Simon Nitinol filter

The Simon Nitinol filter was FDA approved in 1970 and is made of a thermal memory alloy, which makes it pliable at room temperature prior to insertion and rigid at body temperature once in the cava. Pliability at room temp allows for introduction of the catheter through a smaller sheath (Figure 9F), and into the external jugular or brachial veins. It is also nonferromagnetic, and thus, MRI compatible. This filter is made of two components—a top umbrella-shaped filter mesh is attached to an anchoring basal component. The basal component has small hooks that allow for attachment to the wall of the cava (Figure 9D). The advantage of this filter is the ability to trap smaller emboli compared to other filters. Athanasoulis, et al., reported the lowest rate of recurrent PE with this filter (3%). A recurrence rate of 4.4% was reported in a long-term follow up study by Poletti, et al. However, key disadvantages include a higher incidence of access site and symptomatic IVC thrombosis.

Bird’s Nest filter

The Bird’s Nest filter was introduced in 1982 and revised in 1986. It is composed of 4 long stainless steel wires, each of which is preshaped with many nonmatching bends of short radius. These wires are then attached to V-shaped struts, which anchor the filter to the cava wall (Figure 9F). A later revised version allowed for a larger filter size (from an 8F to a 12F catheter system), permitting placement into larger diameter IVCs. Advantages include lower rates of access site and IVC thrombosis. Although some studies have shown lower recurrence rates of PE (3% and 2.7%), a higher PE recurrence rate of 7% was demonstrated in a study by Athanasoulis, et al. Disadvantages include difficult placement and MRI incompatibility.

TrapEase filter

The TrapEase filter was cleared by the FDA in 2000. It is trapezoid-shaped and made up of 2 baskets that are attached to 6 side struts. Distal hooks at each end of the side struts allow for filter anchoring (Figure 9G). It is composed of nitinol material, making it MRI compatible. This filter has a small and long delivery system (8F), thus, permitting placement via the antecubital approach. A multicenter trial conducted by Rousseau, et al., showed a zero recurrence rate of PE in 65 patients at 6 months postplacement.

Retrievable IVC filters

Four retrievable IVC filters are described—all of which have been cleared by the FDA for use in the United States. With the exception of the OptEase filter, all have been cleared for use as permanent and retrievable filters. They are inserted via the femoral or right internal jugular approach, and they share similar complication rates with permanent filters. Their indications and contraindications are similar to those for permanent filters. However, as implied by their name, they can be retrieved following placement.

Retrieval of the filters has been shown to be safe, with few immediate or late complications. Failures at filter removal are usually attributed to incorporation of the filter into the wall of the cava, significant filter tilt, and large clot burden. Removal of a filter once it has been incorporated into the vessel carries significant risk of traumatic bleed, and significant filter tilt makes it difficult to adequately engage the filter during retrieval.

Gunther Tulip filter

The FDA first approved the Gunther Tulip filter for use as a permanent filter in 2001, and later as a retrievable filter in 2003. This filter utilizes 4 struts, configured as a cross, that form a half basket with hooks at each end of each strut. These hooks attach the filter to the caval wall. There is a hook at the caudal aspect of the filter, which facilitates retrieval (Figure 10A). It is composed of a nonferromagnetic coni-chrome, which is MRI compatible, and is generally introduced via the right IJ approach.

Although multiple studies have demonstrated successful retrieval, a precise time frame for successful clinical retrieval has yet to be defined. A recent study by Smouse, et al., showed reliable retrieval rates at 12 weeks, with successful retrieval up to 17 months after implantation. Complications of the Gunther Tulip filter have been attributed to problems with deployment, damage to adjacent structures, and repeat thrombosis. In a study by Looby, et al, 2.72% (4/147) of patients developed pneumothoraces secondary to jugular puncture for filter deployment,
single instances of an asymptomatic IVC filter perforation, as well as incomplete filter expansion and one episode of breakthrough pulmonary embolus were reported (0.68%).

G2 filter

The G2 filter is an evolution of the original Recovery Option filter (Figure 10C), which is no longer available for use as a retrievable filter in the United States. It was approved by the FDA in 2005 for use as a permanent filter, and later approved as a temporary filter in 2008. This filter is composed of 12 nitinol wires that join together at the apical end. Six short, upper wires act as stabilizing arms that contact the wall of the IVC, and the remaining 6 have longer wires with hooks at their tips for further anchoring of the filter (Figure 10B). It is MRI compatible, and is introduced via the right IJ approach. In a retrospective study by Kim, et al., in 2000, there was a 6.5% (5/77) rate of symptomatic PE recurrence.

OptEase filter

This filter was approved by the FDA as a retrieval/optional filter in 2002. It shares a similar design to the TrapEase (permanent) filter, and is made up of a single nitinol metal tube with a double basket design. The basket-like configuration is connected by six straight struts between the proximal and distal ends. There are unidirectional barbs at the superior aspect of the 6 struts that aid in anchoring the filter in the IVC (Figure 10D). Once deployed, the filter imparts an outward radial force on the luminal surface of the cava to ensure appropriate positioning and stability. Unique to the OptEase is the option for femoral retrievability, which is facilitated by the unidirectional barbs and a hook at the caudal end of the filter. It is MRI compatible.

In a single-institution clinical study by Keller IS, 83 patients received OptEase filters, 58 of which (70%) were removed in a mean time of 13.8 days. No symptomatic PE occurred during this time, and after a mean follow-up period of 3.5 years, only one incident of late caval thrombosis was documented. A multicenter study by Rosenthal evaluated 40 patients who received OptEase filters. The filter was successfully removed in all patients, and no symptomatic PE, caval thrombosis, or filter damage was demonstrated. The PROOF trial assessed the OptEase filter’s safety and efficacy as a permanent filter. From a cohort of 150 patients, 149 had successful filter implantation. Over the course of the study, major adverse events were reported in 39 patients (26%); however, 38 of these were deaths prior to the end of the study that were determined to be unrelated to the presence of the filter or the deployment procedure. The rates of filter migration and symptomatic thrombosis at one month were 0.9% and 0.8%, respectively, and they remained stable at a 6-month follow-up.

Celect filter

The Celect filter, approved by the FDA in 2008, shares a similar design with the Gunther Tulip filter. Four primary struts serve as anchoring legs, along with 8 independent secondary struts that provide additional clot trapping capabilities (Figure 10E). This configuration serves to center the filter and prevent tilt, and allows improved filter removal if any of the struts become incorporated into the IVC wall. Insertion is made either via the femoral or IJ approach. It is also MRI compatible.

Choice of permanent vs. retrievable filters

It has become a growing trend in the United States not to remove retrievable filters once they have been placed. A retrospective review by Gaspard in 2009 showed only 11 (3.7%) of 298 retrievable filters were removed after placement during a 3-year period from January 2004 to December 2006. A retrospective study conducted by Janne d’Othee, et al., evaluated multiple reasons for retrievable filter placement and lack of removal, and showed that it was only cost effective to place retrievable filters in patients < 65 years and those without ongoing malignancy. According to the Society of Interventional Radiology guidelines, the decision to place either permanent or retrievable/optional filters should be made on the anticipated required duration of protection against clinically significant PE and/or risk of pharmacologic therapy.

Conclusion

Pulmonary embolus resulting from DVT results in significant morbidity and mortality, resulting in the need for adequate prevention and treatment. Although systemic anticoagulation therapy remains the initial and most effective treatment, inferior vena cava filters play a pivotal role in preventive management in patients with established DVT and/or PE, as well as in adequate prophylaxis of patients at high risk of thrombosis. A variety of these filters are FDA approved and available today; most are relatively safe. Most filters placed within the past several years are designated as retrievable, although the vast majority of these have actually not been removed. The choice of using a
particular filter should be made with careful consideration of the duration of intended use, inherent characteristics of the filter, and the associated complications.

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